Noise Assumptions in Complex-Valued SENSE MR Image Reconstruction

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OUTLINE

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Motivation

In MRI k-space for images is not measured instantaneously.

In parallel imaging, sub-sampled k-space points are measured in parallel and combined to form a single image.

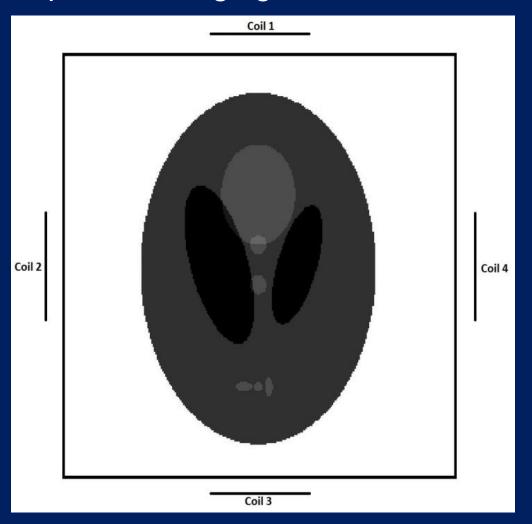
Image and volume measurement time is decreased at the expense of increased image reconstruction difficulty and time.

The SENSE parallel imaging reconstruction technique utilizes a complex-valued least squares estimation process.

However, in SENSE the covariance is not properly modeled.

Background

In parallel imaging there is more than one receive coil.



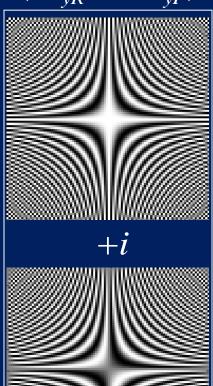
Each coil measures a *k*-space array that is reconstructed into an aliased image then combined to form a single unaliased image.

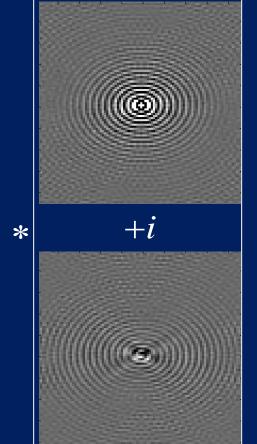
Background

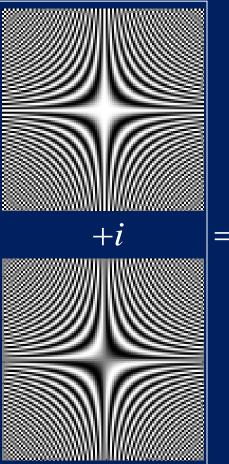
Image inverse Fourier Reconstruction for single coil.



 $\overline{(\Omega_{yR} + i\Omega_{yI})} * (F_R + iF_I) * (\Omega_{xR} + i\Omega_{xI})^T = (V_R + iV_I)$





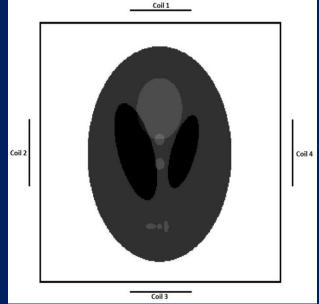


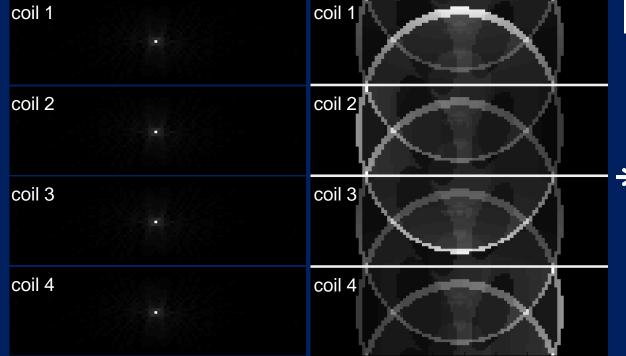


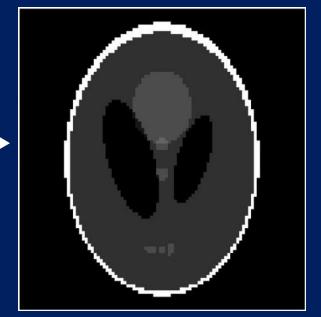
Rowe, Marquette U

Background

Each coil measures a *k*-space array that is reconstructed into an aliased image then combined to form a single image.



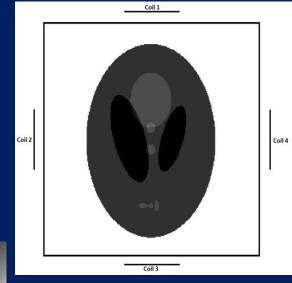


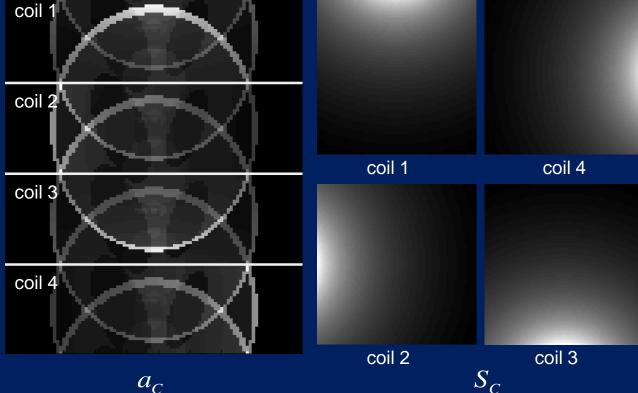


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Background

Each coil measures a *k*-space array that is reconstructed into an aliased image then combined to form a single image.







 v_{c}

The SENSE model for aliased voxel values from n coils is

$$a_{C} = S_{C} v_{C} + \varepsilon_{C} , \varepsilon_{C} \sim CN(0, \Psi_{C})$$
 $n \times 1 n \times 1$

where for each voxel

$$\Psi_C = \Psi_R + i\Psi_I$$

 a_C is a vector of the n complex-valued aliased voxel values

 v_C is a vector of the A unaliased voxel values

$$a_C = a_R + ia_I$$

$$v_C = v_R + iv_I$$

 S_C is an nxA matrix of complex-valued coil sensitivities

$$S_C = S_R + iS_I$$

 ε_C is a vector of the n complex-valued error values

$$\varepsilon_C = \varepsilon_R + i\varepsilon_I$$

The SENSE process

$$a_C = S_C v_C + \varepsilon_C, \quad \varepsilon_C \sim CN(0, \Psi_C)$$
 $n \times 1 n \times A A \times 1 n \times 1 \quad \Psi_C = \Psi_R + i\Psi_L$

uses the complex normal distribution

$$f(\varepsilon_C) = (2\pi)^{-n} \left| \Psi_C \right|^{-1} e^{-1/2\varepsilon_C^H \Psi_C^{-1} \varepsilon_C}, \quad H \text{ is the conjugate transpose (Hermetian)}$$

and for N_C coil measurements

$$f(a_C) = (2\pi)^{-n} |\Psi_C|^{-1} e^{-1/2(a_C - S_C v_C)^H \Psi_C^{-1}(a_C - S_C v_C)}$$

From the distribution for the *n* coil measurements

$$f(a_C) = (2\pi)^{-n} |\Psi_C|^{-1} e^{-1/2(a_C - S_C v_C)^H \Psi_C^{-1}(a_C - S_C v_C)}$$

the voxel values can be estimated as

$$\nu_C = (S_C^H \Psi_C^{-1} S_C)^{-1} S_C^H \Psi_C^{-1} a_C$$

with knowledge of S_C and Ψ_C .



Instead of writing the model with complex numbers as

$$a_{C} = S_{C} v_{C} + \mathcal{E}_{C},$$
 $n \times 1 n \times A A \times 1 n \times 1$

$$a_C = a_R + ia_I$$
 $S_C = S_R + iS_I$ $v_C = v_R + iv_I$ $\varepsilon_C = \varepsilon_R + i\varepsilon_I$

we can write the model using an isomorphism as

$$a = S v + \varepsilon$$
 $2n \times 1$
 $2n \times 2A \times 1$
 $2n \times 1$

$$a = \begin{pmatrix} a_R \\ a_I \end{pmatrix} \qquad S = \begin{pmatrix} S_R & -S_I \\ S_I & S_R \end{pmatrix} \quad v = \begin{pmatrix} v_R \\ v_I \end{pmatrix} \qquad \varepsilon = \begin{pmatrix} \varepsilon_R \\ \varepsilon_I \end{pmatrix}$$

Pruessmann et al.: SENSE: Sensitivity Encoding for Fast MRI. MRM 42:952–962, 1999. Wooding The multivariate distribution of complex normal variables. Biometrika 43:212–215, 1956. Bruce and Rowe: In progress.

Then the distribution for n coil measurements is

$$f(a) = (2\pi)^{-n} |\Psi_{SE}|^{-1/2} e^{-1/2(a-Sv)'\Psi_{SE}^{-1}(a-Sv)}$$

with

$$a = \begin{pmatrix} a_R \\ a_I \end{pmatrix} \qquad S = \begin{pmatrix} S_R & -S_I \\ S_I & S_R \end{pmatrix} \quad v = \begin{pmatrix} v_R \\ v_I \end{pmatrix} \qquad \varepsilon = \begin{pmatrix} \varepsilon_R \\ \varepsilon_I \end{pmatrix}$$

and the complex normal distribution imposes skew-symmetric

$$\Psi_{SE} = \begin{pmatrix} \Psi_R & -\Psi_I \\ \Psi_I & \Psi_R \end{pmatrix}$$

The skew-symmetric covariance structure

$$\Psi_{SE} = \begin{pmatrix} \Psi_R & -\Psi_I \\ \Psi_I & \Psi_R \end{pmatrix} \text{ is incorrect.}$$

What this says is that cov(I, I) = cov(R, R)

and that cov(I, R) = -cov(R, I).

The proper covariance structure should be

$$\Psi_{SI} = \begin{pmatrix} \Psi_R & \Psi_{RI} \\ \Psi'_{RI} & \Psi_I \end{pmatrix}$$

(SE for SENSE and SI for new covariance model SENSE-ITIVE)

Examine the difference between the two covariance structures

$$\Psi_{SE} = \begin{pmatrix} \Psi_R & -\Psi_I \\ \Psi_I & \Psi_R \end{pmatrix} \qquad \Psi_{SI} = \begin{pmatrix} \Psi_R & \Psi_{RI} \\ \Psi'_{RI} & \Psi_I \end{pmatrix}$$

in the distribution

$$f(a) = (2\pi)^{-n} |\Psi_{SE/SI}|^{-1/2} e^{-1/2(a-Sv)'\Psi_{SE/SI}^{-1}(a-Sv)}$$

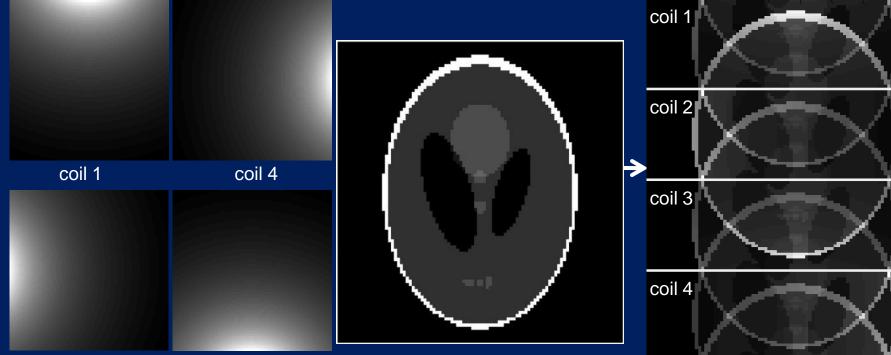
through estimates

$$v_{SE} = (S' \Psi_{SE}^{-1} S)^{-1} S' \Psi_{SE}^{-1} a$$
$$v_{SI} = (S' \Psi_{SI}^{-1} S)^{-1} S' \Psi_{SI}^{-1} a$$

Results

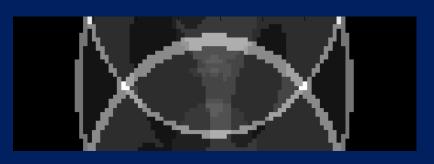
Noiseless multi-coil spatial frequency arrays are with

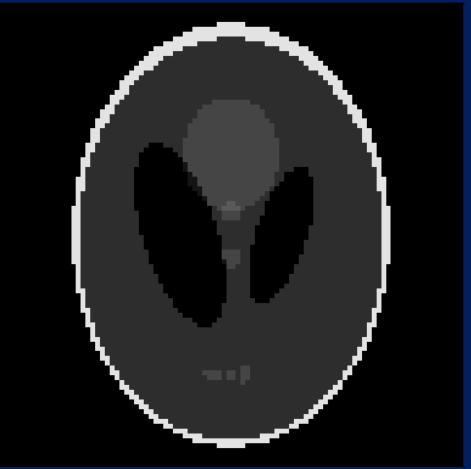
$$\Psi_{SI} = \begin{pmatrix} \Psi_R & \Psi_{RI} \\ \Psi'_{RI} & \Psi_I \end{pmatrix} \qquad \Psi_R = \begin{pmatrix} 1 & .33 & .11 & .33 \\ .33 & 1 & .33 & .11 \\ .11 & .33 & 1 & .33 \\ .33 & .11 & .33 & 1 \end{pmatrix} \Psi_{RI} = \begin{pmatrix} 0 & -.11 & -.07 & -.11 \\ .33 & 0 & -.11 & -.07 \\ .42 & .26 & 0 & -.11 \\ .26 & .42 & .26 & 0 \end{pmatrix}$$



coil 2 coil 3 Bruce and Rowe: In progress.

Results Magnitude

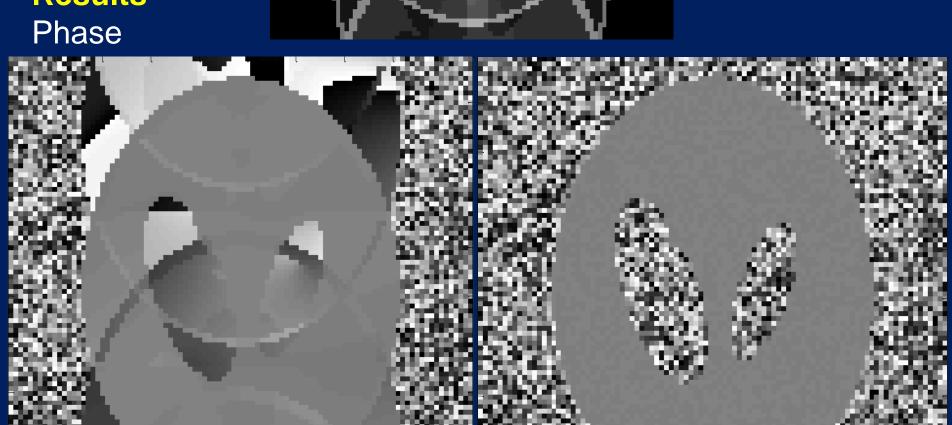




SENSE

SENSE-ITIVE

Results



SENSE

SENSE-ITIVE

Discussion

The SENSE image reconstruction method was described.

The SENSE reconstruction written with an isomorphism.

The covariance structure of complex SENSE described.

New SENSE-ITIVE method described with proper covariance.

Results of SENSE & SENSE-ITIVE reconstruction presented.

Ghosting present in SENSE magnitude and phase images.

Better reconstruction in SENSE-ITIVE reconstruction especially phase used for complex-valued time series activation.

Thank You

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